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**APPLICATION FOR  
UNITED STATES LETTERS PATENT**

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Title: RETINAL TREATMENT METHOD

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**SPECIFICATION**

## RETINAL TREATMENT METHOD

### Field of the Invention

The invention relates to methods for providing a device or composition to a retina.

### Background of the Invention

The retina is the innermost layer of the wall of the eyeball located in the posterior segment of the eye. Developed as an outgrowth from the brain, the retina contains nervous tissue, specifically, light-sensitive cells (photoreceptors) and complex neural networks. These networks provide visual information and send impulses through the optic nerve to the brain.

Degenerative diseases of the retina, such as retinitis pigmentosa, age-related macular degeneration, and hereditary retinal degenerations cause degeneration and death of the photoreceptor cells, resulting in decreased visual function. Fortunately, even in end-stage disease, numerous neuronal cells in the inner retina survive. However, because of loss of the photoreceptors, light stimulation does not occur and the neuronal cells must be artificially stimulated to restore some degree of visual function.

The neuronal cells may be stimulated, either from the outer surface of the retina or from the so-called subretinal space. One technique for subretinal stimulation uses semiconductor microphotodiode arrays (SMA) as described in Peyman et al., Ophthalmic Surgery and Lasers, 1998, vol. 29, p. 234, which is expressly incorporated by reference herein in its entirety. These arrays are fabricated by standard photomask and etch techniques, and can be produced with thicknesses ranging from about 10-200  $\mu\text{m}$  and sizes varying from about 0.5-5 mm in diameter. The arrays are separated into subunits, which create a pixel density of over 1000 subunits/ $\text{mm}^2$ . The subunits have no electrical connection; they are powered by incident light having a wavelength between 500-1100 nm. Another technique for retinal stimulation uses an electrode array to electrically stimulate the neurofiber layer of the retina. The array has 25 platinum disks arranged in a 5x5 square, as reported by Majji et al., Investigative Ophthalmology and Visual Science, 1999, vol. 40, p. 2073. The improved surface of the platinum disk forms a planar array of stimulating electrodes in a silicon matrix that is less than 1 mm thick. Twenty-five wires originating from the disk form a cable which extends from the array and is at least 10 cm long and 600  $\mu\text{m}$  thick. To implant the array into the eye, the surface of the implant (3x5 mm) is placed over and is fixed to the retina either by mechanical fasteners such as pins or tacks, or by bioadhesives.

There are, however, several disadvantages of implanting the aforementioned types of arrays into the subretinal space. One disadvantage is that the implant may interfere with nutrition of the retina, since nutrients come partially from the choroid (the back of the retina). Fenestrations, or small

openings in the array, can help to maintain nutrient accessibility to the retina. Implanting the electrode type of array over the surface of the retina has additional drawbacks. One drawback is that fixing the array over the retina is very difficult. If pins or other mechanical fasteners are used, they should  
5 penetrate the entire retina and reach the scleral wall in order to secure the array, but this increases the risk of hemorrhage from the retinal and choroidal circulation. The increased fibrous proliferation around both the fasteners and the array also causes localized scarring and traction on the retina. Another disadvantage is that electrical stimulation in the subretinal space may not  
10 adequately excite the ganglion cells and the neurofiber layer, which are located in the outer portion of the retina.

Drugs such as gancyclovir or various steroids can also be administered to the patient to attempt to prevent, halt, or alleviate the pathological process. Ocular drugs may be administered systemically,  
15 parenterally, or topically. Alternatively or additionally, the drugs may be administered in a slow release formulation.

While current methods exist for treating patients experiencing a loss in visual function due to retinal pathology, several problems still remain. Thus, additional methods to improve visual function, while decreasing or  
20 eliminating these problems, are desirable.

#### Summary of the Invention

The invention relates to a method to provide an interventional or therapeutic substance to patients who have experienced decreased visual function due to retinal pathology or injury. The invention is also directed to a

method for treating or preventing retinal pathology or injury in a mammal by surgically affixing a therapeutic or preventive substance under an internal limiting membrane in the eye to contact and stimulate the retina.

5 The inventive method provides the retinal stimulator substance to a mammalian eye by visualizing the internal limiting membrane of the eye, locating the retinal stimulator between the internal limiting membrane and the retina, and securing the substance under the internal limiting membrane. The method thus locates, contains, and secures a retinal stimulator substance in proximity to the retina, all by using a space provided by the internal limiting  
10 membrane in the eye.

In one embodiment, the substance is an array that is photostimulated to excite the retina. In another embodiment, the substance is an array that is electrically stimulated to excite the retina. In yet another embodiment, the substance is a drug that directly or indirectly stimulates the retina, for example, a drug that is formulated in a vehicle for slow-release  
15 delivery.

The inventive method takes advantage of the physiological placement of the internal limiting membrane in the eye. Previous surgical implant methods had removed the internal limiting membrane. However, the  
20 inventive method not only retains the internal limiting membrane, but also takes advantage of the space between it and the adjacent retinal layers to implant a therapeutic or preventative substance. In this way, non-physiological mechanical or chemical fasteners are not needed to locate and secure the implanted substance in place. Thus, there are no devices or compositions which

may cause bleeding from the choroid or which may promote retinal traction originating from the cells migrating from the choroid through the mechanical pins, both of which are problems in current methods.

Another improvement using the inventive method is that the substance implanted is in direct contact with the neurofiber layer and ganglion cells of the retina. This advantageously enhances their stimulation, since the distance between the substance and its target is decreased. For example, when electrical arrays are implanted, there is enhanced qualitative and quantitative cell stimulation because the stimulus is close enough to reach ganglion cells and the neurofiber layer that is located a distance of about 10-50  $\mu\text{m}$  away.

Still another improvement is that the inventive method eliminates the need for external stimulation, as is used with currently available diode arrays.

These and other advantages will be apparent from the following figures and detailed description.

#### Brief Description of the Drawings

FIG. 1 is a schematic cross-sectional view of a mammalian eye.

FIG. 2 is an enlarged diagrammatic illustration of the circled area 2 of FIG. 1 showing detailed retinal and choroid structures and placement of a substance using the inventive method.

#### Detailed Description

With reference to FIG. 1, a mammalian eye 10 is shown. The locations of the vitreous cavity 8, posterior chamber 9, anterior chamber 11, cornea 12, conjunctiva 13, iris 14, optic nerve 15, sclera 16, macula lutea 17, lens 18, retina 20, ora serrata 21, and choroid 22 are illustrated.

The most sensitive portion of the retina 20 is the macula lutea 17, which is located in the center of the posterior part of the retina 20. The inner surface of the retina 20, near the border of the optic nerve 15, has a shallow round depression, the fovea 41. The fovea 41 is surrounded by the central area, distinguished by the great number of ganglion cells and by the general refinement and even distribution of the structural elements, especially the rod cells and the cone cells. About one-tenth inch inside the fovea 41 is the point of entrance of the optic nerve 15 and its central artery. At this point, the retina 20 is incomplete and forms the blind spot.

With reference to FIG. 2, the retina 20 forms the innermost layer of the posterior portion of the eye and is the photoreceptor organ. The retina 20 has an optical portion that lines the inner surface of the choroid 22 and extends from the papilla of the optic nerve 15 to the ora serrata 21 anteriorly. At the papilla, where the retina 20 continues into the tissue of the nerve 15, and at the ora serrata 21, the retina 20 is firmly connected with the choroid 22. The retina 20 has ten parallel layers which are, from outside to inside, as follows: the pigment epithelium 101, photoreceptor cells (rod cells and cone cells) 102, the outer limiting membrane 103, the outer nuclear layer 104, the outer plexiform layer 105, the inner nuclear layer 106, the inner plexiform layer 107, the layer of ganglion cells 108, the layer of optic nerve fibers or neurofiber layer 109, and the so-called inner limiting membrane 110. The inner limiting membrane 110 is very thin (less than 5  $\mu$ m), and normally adheres with the neurofiber layer 109 of the ganglion cells 108.

The inventive method takes advantage of the adjacent positions of the neurofiber layer 109 and ganglion cells 108 with the inner limiting membrane 110 to provide a space 120 into which a substance 130 for treating the retina 20, such as an array for electrostimulation of the retina, can be implanted and secured. The potential for and use of this space 120 in implanting an array or any other material has heretofore been unrecognized and unappreciated.

In the method, the patient is prepared for surgery, typically by providing a topical anesthesia to the eye and dilating the pupil. The eyeball is exposed and the vitreous is removed from the vitreous cavity 8 by standard techniques known to one skilled in this art. The internal limiting membrane 110 is then rendered visible to the surgeon, typically by staining. Any water soluble stain which stains the basement membrane of the internal limiting membrane 110 can be used, for example, indocyanine green, trypan blue, methylene blue, etc. The stain, for example one or two drops, is placed into the eye to allow visualization of the internal limiting membrane 110. A small incision, typically less than about 0.5 mm in diameter, is made into the internal limiting membrane 110 in the area of the macula lutea 17.

In current methods for treating a macular hole, the internal limiting membrane 110 is separated and removed using forceps.

To create a space where an array can be placed under the internal limiting membrane 110, the internal limiting membrane 110 can be separated from the retina 20 by a blunt-tipped spatula or a cannula for injection of a liquid.



In the inventive method, however, instead of cutting and removing the internal limiting membrane 110 as is routinely done, the internal limiting membrane 110 is left in place and is, in fact, used to locate the implanted substance 130. A small incision 132 is made in the internal limiting membrane 110, and the membrane 110 is then separated from the adjacent neurofiber layer 109. The substance 130 is implanted, and because the incision used for separation of the internal limiting membrane is small, the substance 130 is inserted in a secure fit. The internal limiting membrane is then repositioned over the substance 130. Furthermore, the repositioned internal limiting membrane 110 also secures the implanted substance 130 to the neurofiber layer 109 and ganglion cells 108. After the substance 130 is located and secured under the internal limiting membrane 110, the vitreous cavity 8 can be re-filled with fluid, for example, air. This fluid is subsequently absorbed and is replaced by body fluids.

In the inventive method, positioning and replacement of the internal limiting membrane 110 over the implanted substance 130 either eliminates the need for an adhesive, or allows a smaller quantity of adhesive to be used than if the internal limiting membrane was removed. If desired, however, an adhesive can also be applied to close the incision, but is not placed between the substance 130 and the retina 20. The adhesive can be, for example, a commercial fibrin sealant, autologous fibrin, Cell-Tak, photocurable glues, polyethylene glycol hydrogels, as described in Margalit et al., Retina, 2000, vol. 20, p. 469, which is expressly incorporated by reference herein in its entirety.

If the substance 130 implanted is an array, it may be with or without external connections. For example, an array with electrode connectors having a length of about 50  $\mu\text{m}$  to about 100  $\mu\text{m}$  may be implanted. An array can be of any type as is known to one of skill in this art, such as the semiconductor microphotodiode array that is described by Peyman et al., Ophthalmic Surgery and Lasers, 1998, vol. 29, p. 234, which is expressly incorporated by reference herein in its entirety. An array as small as 10  $\mu\text{m}$  can be implanted. Alternatively, multiple small arrays, with a total size of up to about 8 mm, may be implanted. Their position can subsequently be organized and oriented magnetically. The array can be fabricated to be fenestrated, or it can be without fenestrations. The individual array can be positive-intrinsic layer-negative (PiN), mixed, negative-intrinsic layer-positive (NiP), or uniform. In the array, light absorption occurs in the front and the electricity runs to the side or the back. If electrode arrays are used, the technology described by Majji et al. is utilized, with connectors to penetrate the neurofiber layer 109 of the retina 20.

The retinal stimulator substance 130 may also be a drug. As one example, the drug may be an  $\alpha$ -adrenergic agonist or a  $\beta$ -adrenergic agonist, as disclosed in United States Patent No. 6,066,675 which is expressly incorporated by reference herein in its entirety. As other examples, the drug may be one or more antiinflammatory agents and/or antiproliferative agents, as is known to one skilled in the art. The drug may be implanted either alone or may be incorporated into a drug delivery system, such as a slow-release system or formulation. Examples of such systems are known to one of skill in this art and

include, but are not limited to, a capsule, a bead, a liposome, a sphere, and/or a dissolvable biocompatible polymer sheet.

The inventive method provides several advantages. It eliminates the need for surgical removal of the internal limiting membrane 110.

5 Furthermore, the inventive method takes advantage of the presence of the internal limiting membrane 110 to provide a "pocket" or space 120 for implanting the substance 130. If the substance 130 is an array, the approximation of the array to the ganglion cells 108 and the neurofiber layer 109 can better amplify the stimulation of these structures. The array thus placed requires less electrical  
10 power than is required with arrays implanted by previously known methods such as using adhesives. The signal generated, being located directly adjacent its retinal target site, is less likely to be attenuated and hence will be more efficacious. The array 130 is also securely maintained in the space 120 without the need for either mechanical fixatives, such as retinal tacks, or chemical  
15 fixatives, such as adhesives. This eliminates the problems of bleeding and/or tearing that are known to occur when mechanical fasteners such as tacks or pins are used. The inventive method also eliminates the problems associated with the use of adhesives, namely, that adhesives come off and the substance becomes dislodged from its original site of implantation, and that adhesives  
20 serve as insulators and hence interfere with transmission of an electrical signal from an array to the retina 20.

It should be understood that the embodiments of the present invention shown and described in the specification are only preferred embodiments of the inventor who is skilled in the art and are not limiting in any

What is claimed is: